

# Mechanisms of Beat-to-Beat Regulation of Cardiac Pacemaker Cell Function by $\text{Ca}^{2+}$ Cycling Dynamics

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**ABSTRACT** Whether intracellular  $\text{Ca}^{2+}$  cycling dynamics regulate cardiac pacemaker cell function on a beat-to-beat basis remains unknown. Here we show that under physiological conditions, application of low concentrations of caffeine (2–4 mM) to isolated single rabbit sinoatrial node cells acutely reduces their spontaneous action potential cycle length (CL) and increases  $\text{Ca}^{2+}$  transient amplitude for several cycles. Numerical simulations, using a modified Maltsev-Lakatta coupled-clock model, faithfully reproduced these effects, and also the effects of CL prolongation and dysrhythmic spontaneous beating (produced by cytosolic  $\text{Ca}^{2+}$  buffering) and an acute CL reduction (produced by flash-induced  $\text{Ca}^{2+}$  release from a caged  $\text{Ca}^{2+}$  buffer), which we had reported previously. Three contemporary numerical models (including the original Maltsev-Lakatta model) failed to reproduce the experimental results. In our proposed new model,  $\text{Ca}^{2+}$  releases acutely change the CL via activation of the  $\text{Na}^+/\text{Ca}^{2+}$  exchanger current. Time-dependent CL reductions after flash-induced  $\text{Ca}^{2+}$  releases (the memory effect) are linked to changes in  $\text{Ca}^{2+}$  available for pumping into sarcoplasmic reticulum which, in turn, changes the sarcoplasmic reticulum  $\text{Ca}^{2+}$  load, diastolic  $\text{Ca}^{2+}$  releases, and  $\text{Na}^+/\text{Ca}^{2+}$  exchanger current. These results support the idea that  $\text{Ca}^{2+}$  regulates CL in cardiac pacemaker cells on a beat-to-beat basis, and suggest a more realistic numerical mechanism of this regulation.

## INTRODUCTION

Experimental studies of the last two decades have established that intracellular  $\text{Ca}^{2+}$  signaling contributes to regulation of normal cardiac pacemaker cell function (1–6). Automaticity of the sinoatrial nodal cell (SANC), the primary cardiac pacemaker cells, has been suggested (7) to be regulated by a system of two clock-like oscillators: the sarcoplasmic reticulum (SR), acting as a  $\text{Ca}^{2+}$  clock, rhythmically discharges diastolic local  $\text{Ca}^{2+}$  releases (LCRs) beneath the cell surface membrane; and LCRs activate an inward  $\text{Na}^+/\text{Ca}^{2+}$  exchanger current ( $I_{\text{NCX}}$ ) that accelerates diastolic depolarization (DD) and prompts the surface membrane-clock (M clock), an ensemble of sarcolemmal electrogenic molecules, to generate an action potential (AP) (Fig. 1). Because the M clock regulates SANC  $\text{Ca}^{2+}$  influx and efflux, it also regulates the  $\text{Ca}^{2+}$  clock, forming a coupled-clock system (8,9). The coupled-clock system hypothesis is continually being rigorously debated (10,11) and experimentally challenged (12). Therefore, in this article we provide additional experimental and numerical validation of the coupled clock pacemaker cell concept.

Specifically, we had previously demonstrated that membrane potential fluctuations resulting from the LCRs impart an exponential phase to the late DD that controls the SANC chronotropic state (13). However, in that study, noise characteristics of the membrane potential and LCRs were compared at a given steady state as averaged values over several beats (rather than in a given beat). Our more recent measurements using a high-speed camera demonstrated that

spontaneous, beat-to-beat AP cycle variations are linked to the characteristics of the entire LCR ensemble in any, given cycle (14). The idea of dynamic (beat-to-beat) interactions of the two clocks that ultimately determine the duration of each AP cycle length (CL) has been also validated, in part, by a demonstration that acute flash-induced  $\text{Ca}^{2+}$  release from an intracellular caged buffer (NP-EGTA) produces acute changes in intracellular  $\text{Ca}^{2+}$  dynamics, which result in instantaneous changes in the CL (15). However, in that study, before the flash was applied, SANCs were exposed to artificial  $\text{Ca}^{2+}$  buffering that had substantially prolonged the initial CL beyond physiological range. Therefore, additional studies are required to demonstrate beat-to-beat regulation of CL under physiological conditions. Moreover, specific mechanisms describing how each clock entrains the other remain unknown and require a dedicated numerical investigation. Specifically, it remains unknown, how the membrane  $\text{Ca}^{2+}$ -dependent molecules are affected by release of  $\text{Ca}^{2+}$  in a beat-to-beat manner in response to  $\text{Ca}^{2+}$  perturbation, and how the  $\text{Ca}^{2+}$ -induced M clock changes entrain the  $\text{Ca}^{2+}$  clock.

This study tested whether intracellular  $\text{Ca}^{2+}$  release can regulate the AP firing rate in a beat-to-beat manner at a physiological AP firing rate. To this end, we acutely applied (brief application) low concentrations of caffeine (2–4 mM) onto spontaneously beating SANC, via a picospritzer, to acutely increase open probability of their SR  $\text{Ca}^{2+}$  release channels (RyR) (Fig. 1). To accurately interpret the experimental results and to gain mechanistic insight into the beat-to-beat  $\text{Ca}^{2+}$  regulation of CL, we performed a detailed numerical investigation of these effects. Surprisingly, we found that the experimental results cannot be reproduced

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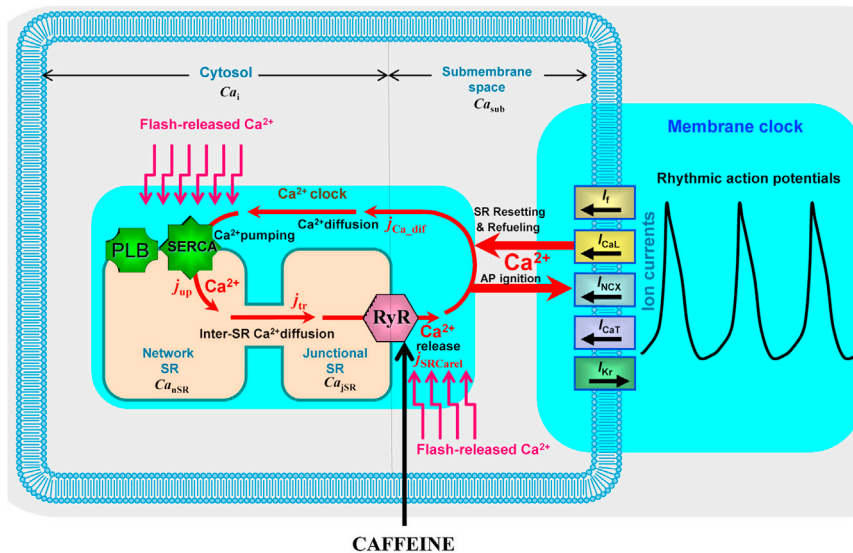


FIGURE 1 Schematic illustrations of the coupled-clock system. In our experimental results and numerical model simulations, the interplay of sarcoplasmic reticulum  $\text{Ca}^{2+}$  cycling proteins and ion channels in SANC is perturbed by either flash-induced  $\text{Ca}^{2+}$  release (zigzag arrows) or by caffeine-induced  $\text{Ca}^{2+}$  release (solid arrow).

by any existing models of the rabbit SA node cell, such as the model of Kurata et al. (16), the original Maltsev-Lakatta coupled-clock model (17), and its updated version by Severi et al. (18). Our proposed new model (modification of the Maltsev-Lakatta model) functionally reproduced the new experimental data, and provided more realistic numerical mechanisms underlying cardiac pacemaker function.

## MATERIALS AND METHODS

### Cell preparation

Single SANCs were isolated from New Zealand White rabbit hearts as previously described in Vinogradova et al. (19). The experiment protocols have been approved by the Animal Care and Use Committee of the National Institutes of Health (protocol No. 034LCS2013). The dissociated cells were stored at  $4^{\circ}\text{C}$  and were used within 8 h of isolation.

### Confocal imaging of AP-triggered $\text{Ca}^{2+}$ transients

SANCs were placed in a laminated chamber ( $25\ \mu\text{g/mL}$ ; Invitrogen, Carlsbad, CA) on an inverted microscope and were loaded with  $5\ \mu\text{M}$  Fluo-4AM (Molecular Probes, Eugene, OR) (see below for details), and subsequently superfused with a Tyrode's solution with the following composition: 140 mM NaCl, 5.4 mM KCl, 2 mM  $\text{MgCl}_2$ , 5 mM HEPES, 1.8 mM  $\text{CaCl}_2$ , and 5.5 mM Glucose, titrated to pH 7.4 with NaOH.  $\text{Ca}^{2+}$  fluorescence was imaged on a LSM510 confocal microscope (Carl Zeiss, Oberkochen, Germany) using a  $40\times/1.3\ \text{N.A.}$  oil immersion lens. Cells were excited with the 488-nm light of an argon laser, and fluorescence emission was collected with a long-pass 505-nm filter. All images were recorded with a scan line ( $512 \times 1$  pixels at  $14.9\ \mu\text{m}$  and 2 ms/line) oriented across the cell length, and processed with the software MATLAB (The MathWorks, Natick, MA). All measurements of  $\text{Ca}^{2+}$  signals were conducted at  $35 \pm 0.5^{\circ}\text{C}$ . The CL was measured as the time period between subsequent  $\text{Ca}^{2+}$  transient peaks. Because each AP induces a  $\text{Ca}^{2+}$  transient, the AP cycle length and  $\text{Ca}^{2+}$  transient cycle length are extremely close to each other, as demonstrated by our simultaneous recordings of APs and  $\text{Ca}^{2+}$  transients (see Fig. S1 in the Supporting Material). In other words, the CL can be accurately measured using recordings of  $\text{Ca}^{2+}$  transients induced by APs.

### Acute caffeine application

We employed a brief rapid application of caffeine onto the cell by pressure-ejection (using a picospritzer) via a nearby pipette. Two types of caffeine experiments were performed in this study. One set of experiments utilized high caffeine concentrations of 10 mM (for 1 s) to induce  $\text{Ca}^{2+}$  transients to assess the SR  $\text{Ca}^{2+}$  content. For these experiments, nine SANCs from three rabbits were used. Another set of experiments utilized lower caffeine concentrations of 2–4 mM (for 1 s) to test the instant effect of caffeine on the spontaneous rate and other characteristics of AP-induced  $\text{Ca}^{2+}$  transients. For these experiments, 11 SANCs from four rabbits were used. To decrease the washout time, the injection glass pipette was mounted so that the caffeine injection flow was oriented in the direction of the chamber solution flow. Further, during caffeine application the bath perfusion rate was increased to 1.5 mL/min to rapidly wash out the caffeine. Our rough estimate using a colored solution and observation of movement of small debris particles near the cells during perfusion indicate that the washout time could be as long as 1 s, giving a total caffeine exposure of  $\sim 2$  s, as numerically modeled (described below).

### Loading SANC with caged $\text{Ca}^{2+}$ buffer NP-EGTA and $\text{Ca}^{2+}$ indicator Fluo-4

In experiments testing the effect of NP-EGTA on SR  $\text{Ca}^{2+}$  content, cells were preloaded with both a cell-permeant photolabile chelator of intracellular  $\text{Ca}^{2+}$  NP-EGTA AM ( $15\ \mu\text{M}$ , Invitrogen) and a  $\text{Ca}^{2+}$  indicator Fluo-4 AM ( $5\ \mu\text{M}$ , Invitrogen) for 25 min at room temperature. In experiments testing the effect of low concentration of caffeine, cells were loaded with  $5\ \mu\text{M}$  Fluo-4AM for 20 min at room temperature.

### Modifications to the original Maltsev-Lakatta numerical model of SANC

To simulate the effects of an acute change in  $\text{Ca}^{2+}$  cycling dynamics on CL, we used both the original 2009 Maltsev-Lakatta numerical model of rabbit SANC (17) and its modification. All formulations and parameters of the modified model used in this article are provided in the Supporting Material. In this study, we excluded a nonselective  $I_{\text{si}}$  current, because this current has properties of  $I_{\text{NCX}}$  and  $I_{\text{CaL}}$  and its molecular identity has not been established (see details in Maltsev and Lakatta (20)).  $I_{\text{Ks}}$  was excluded because of its small expression in rabbit SANC. Finally, the amplitudes of both

inward  $\text{Na}^+$  background current ( $I_{\text{bNa}}$ ) and outward  $\text{Na/K-ATPase}$  current ( $I_{\text{NaK}}$ ) were reduced, as recently suggested by Maltsev and Lakatta (20) and DiFrancesco (22). Note that the density of  $I_f$  (the so-called funny current) remained unchanged ( $g_{\text{If}} = 0.15 \text{ nS/pF}$ ). A formal  $I_f$  blockade in our proposed new model increases AP cycle length from 339.7 to 379.7 ms, which is an increase of 11.8% (beating rate decreases from 176.6 to 158 beats per minute, i.e., by 10.5%).

Table S1 in the Supporting Material lists all variables and their initial values. The membrane potential,  $V_m$ , is described as

$$dV_m/dt = -(I_{\text{CaL}} + I_{\text{CaT}} + I_f + I_{\text{Kr}} + I_{\text{to}} + I_{\text{sus}} + I_{\text{NaK}} + I_{\text{NCX}} + I_{\text{bCa}} + I_{\text{bNa}})/C_m. \quad (1)$$

The effects of simulated caffeine- and photo-released  $\text{Ca}^{2+}$  is mediated via a  $\text{Ca}^{2+}$ -dependence of the ion currents incorporated in the simulations. In our proposed new model, only two currents are  $\text{Ca}^{2+}$ -dependent:  $I_{\text{CaL}}$  (via its  $\text{Ca}^{2+}$ -dependent inactivation, variable  $f_{\text{Ca}}$ ; see the Supporting Material) and  $I_{\text{NCX}}$ .

### Approximation of caffeine effect on RyR release kinetics

The RyR  $\text{Ca}^{2+}$  release flux was numerically modeled as previously suggested by Stern et al. (23), further modified by Shannon et al. (24), and used in our modeling of SANC (17) (see the Supporting Material for details):

$$j_{\text{SRCaRel}} = k_s \times O \times (Ca_{\text{jSR}} - Ca_{\text{sub}}), \quad (2)$$

$$k_{\text{CaSR}} = \text{MaxSR} - (\text{MaxSR} - \text{MinSR}) / (1 + (EC_{50\text{-SR}}/Ca_{\text{jSR}})^{\text{HSR}}), \quad (3)$$

$$k_{\text{oSRCa}} = k_{\text{oCa}}/k_{\text{CaSR}}, \quad (4)$$

$$k_{\text{iSRCa}} = k_{\text{iCa}} \times k_{\text{CaSR}}, \quad (5)$$

$$dR/dt = (k_{\text{im}} \times RI - k_{\text{iSRCa}} \times Ca_{\text{sub}} \times R) - (k_{\text{oSRCa}} \times Ca_{\text{sub}}^2 \times R - k_{\text{om}} \times O), \quad (6)$$

$$dO/dt = (k_{\text{oSRCa}} \times Ca_{\text{sub}}^2 \times R - k_{\text{om}} \times O) - (k_{\text{iSRCa}} \times Ca_{\text{sub}} \times O - k_{\text{im}} \times I), \quad (7)$$

$$dI/dt = (k_{\text{iSRCa}} \times Ca_{\text{sub}} \times O - k_{\text{im}} \times I) - (k_{\text{om}} \times I - k_{\text{oSRCa}} \times Ca_{\text{sub}}^2 \times RI), \quad (8)$$

$$dRI/dt = (k_{\text{om}} \times I - k_{\text{oSRCa}} \times Ca_{\text{sub}}^2 \times RI) - (k_{\text{im}} \times RI - k_{\text{iSRCa}} \times Ca_{\text{sub}} \times R). \quad (9)$$

Porta et al. (25) demonstrated that in planar lipid bilayers, caffeine activation of a single RyR2 channel depends on the free  $\text{Ca}^{2+}$  level on both sides of the channel (i.e., in our case on both submembrane  $[\text{Ca}^{2+}]$  and luminal SR  $[\text{Ca}^{2+}]$ ). Because, as of this writing, it is unknown how RyRs are activated by caffeine in intact SANC, we tested three possibilities of caffeine activation of RyR:

1. Via increasing RyR sensitivity to luminal SR  $[\text{Ca}^{2+}]$  (parameter  $EC_{50\text{-SR}}$  in Eq. 3) from 0.45 to 0.225 mM;
2. Via increasing the rate of transition into open state  $O$  from reactivated state  $R$  (parameter  $k_{\text{oCa}}$  in Eq. 4) from 10 to 20  $\text{mM}^{-2} \times \text{ms}^{-1}$ ; and
3. A combination of the above two changes.

### Numerical estimation of the intracellular NP-EGTA concentration

Our formulations for  $\text{Ca}^{2+}$  buffering by NP-EGTA in the cytosol ( $f_{\text{CBi}}$ ) and in the subspace ( $f_{\text{CBsub}}$ ) are as follows:

$$f_{\text{CBi}}/dt = \text{CB}_{\text{on\_rate}} \times Ca_i \times (1 - f_{\text{CBi}}) - \text{CB}_{\text{off\_rate}} \times f_{\text{CBi}}, \quad (10)$$

where  $\text{CB}_{\text{on\_rate}}$  is the  $\text{Ca}^{2+}$  association constant for NP-EGTA,  $\text{CB}_{\text{off\_rate}}$  is the  $\text{Ca}^{2+}$  dissociation constant for NP-EGTA, and  $Ca_i$  is the intracellular  $\text{Ca}^{2+}$  concentration

$$f_{\text{CBsub}}/dt = \text{CB}_{\text{on\_rate}} \times Ca_{\text{sub}} \times (1 - f_{\text{CBsub}}) - \text{CB}_{\text{off\_rate}} \times f_{\text{CBsub}}, \quad (11)$$

where  $Ca_{\text{sub}}$  is the subspace  $\text{Ca}^{2+}$  concentration.

Formulations of  $\text{Ca}^{2+}$  dynamics in cytosolic ( $Ca_i$ ) and subspace ( $Ca_{\text{sub}}$ ) compartments were complemented by flash release flux  $j_{\text{PPs}}$  from caged NP-EGTA as follows:

$$dCa_i/dt = (j_{\text{Ca\_dif}} \times V_{\text{sub}} - j_{\text{up}} \times V_{\text{nSR}})/V_i - (\text{CB}_{\text{Conc}} \times f_{\text{CBi}}/dt + \text{CM}_{\text{tot}} \times df_{\text{CMi}}/dt + \text{TC}_{\text{tot}} \times df_{\text{TC}}/dt + \text{TMC}_{\text{tot}} \times df_{\text{TMC}}/dt) + j_{\text{PPs}}. \quad (12)$$

$$dCa_{\text{sub}}/dt = j_{\text{SRCaRel}} \times V_{\text{jSR}}/V_{\text{sub}} - (I_{\text{CaL}} + I_{\text{CaT}} + I_{\text{bCa}} - 2 \times I_{\text{NCX}})/(2 \times F \times V_{\text{sub}}) - (\text{CB}_{\text{Conc}} \times f_{\text{CBsub}}/dt) + j_{\text{Ca\_dif}} + \text{CM}_{\text{tot}} \times df_{\text{CMs}}/dt + j_{\text{PPs}}. \quad (13)$$

### Simulations using other models

We also tested whether the contemporary models of Kurata et al. (16) and Severi et al. (18) would reproduce effects of caffeine- and flash-induced  $\text{Ca}^{2+}$  release measured experimentally in SA node cells. For this comparison, we performed simulations using the Cellular Open Resource program developed and maintained at Oxford University (<http://cor.physiol.ox.ac.uk>). Cellular Open Resource can run numerous cell models, including these two models, in the CellML format available at <http://www.cellml.org>.

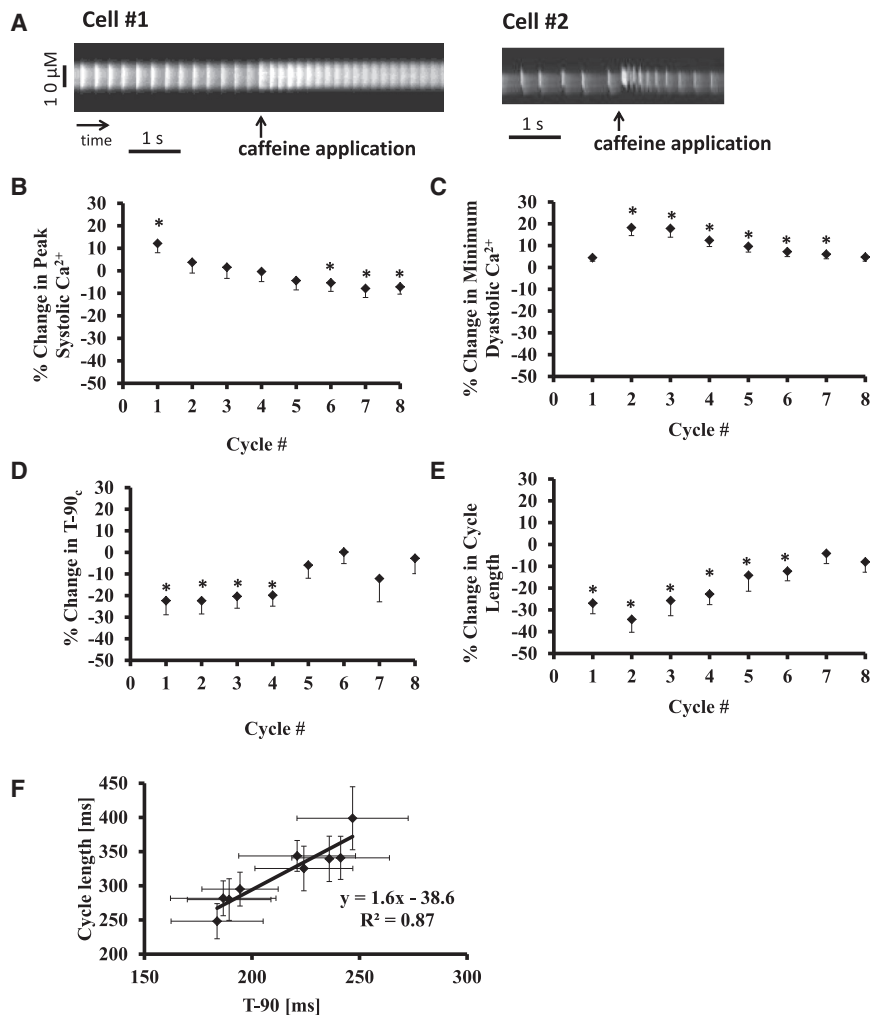
### Statistical analysis

Data are presented as mean  $\pm$  SE. A linear mixed-effects model with Dunnett's method to adjust  $p$  values was used (26). This model accounts for repeated measurements on the same preparation while allowing testing for differences among different beats.  $P < 0.05$  was taken to indicate statistical significance.

## RESULTS

### Rapid application of caffeine affects the $\text{Ca}^{2+}$ transient characteristics and cycle length

Fig. 2 A illustrates representative examples of the effect of caffeine to release  $\text{Ca}^{2+}$  in two SANCs. Caffeine application acutely increased the systolic  $\text{Ca}^{2+}$  transient amplitude (by  $12 \pm 4\%$ ). The caffeine-caused acute effect



**FIGURE 2** Effect of caffeine on the rate of AP-induced  $\text{Ca}^{2+}$  transients. (A) Two representative examples of original recordings of the effect of caffeine on AP-induced  $\text{Ca}^{2+}$  transients. (B–E) Average data obtained in 11 SANs. An acute application of low concentrations (2–4 mM) of caffeine instantly affects peak systolic  $\text{Ca}^{2+}$  signal, minimum diastolic  $\text{Ca}^{2+}$  signal,  $T-90_c$ , and cycle length. (F) Relationship between cycle length and  $T-90_c$ .

ceased over several beats (Fig. 2 B). The diastolic  $[\text{Ca}^{2+}]$  level also acutely increased in response to caffeine by  $5 \pm 2\%$  on the initial beat, but further increased (by  $18 \pm 4\%$ ) on the following beat (Fig. 2 C). The caffeine effect on the diastolic  $\text{Ca}^{2+}$  level vanished during subsequent cycles (see Table S2). Caffeine reduced the 90% decay time of the AP-induced  $\text{Ca}^{2+}$  transient ( $T-90_c$ ) by  $22 \pm 6\%$  (from  $246.7 \pm 25.8$  to  $186.6 \pm 24.5$  ms) (Fig. 2 D). The reduction in  $\text{Ca}^{2+}$  transient  $T-90_c$  on the following beat was similar to that of the initial beat after caffeine application (by  $23 \pm 6\%$  to  $183.7 \pm 21.4$  ms). Table S2 shows that the caffeine effect on  $T-90_c$  vanished after four cycles. Similar reduction trends of the 50% decay time of intracellular  $\text{Ca}^{2+}$  ( $T-50_c$ ) were found; however, these were only marginally significant in the two following beats after caffeine application ( $P = 0.05$  and  $P = 0.0531$ ). The time-to-peak  $T_p$  was not significantly changed by caffeine.

Changes in the AP-induced  $\text{Ca}^{2+}$  transient cycle length were mirror images of the changes in minimum diastolic  $\text{Ca}^{2+}$  (Fig. 2 E). Before caffeine application, SANs gener-

ated spontaneous rhythmic  $\text{Ca}^{2+}$  transients with a cycle length of  $398.8 \pm 46.1$  ms ( $n = 11$ ). The initial effect of caffeine application was to markedly reduce the  $\text{Ca}^{2+}$  transient cycle length by  $27 \pm 5\%$  (to  $281.7 \pm 25.5$  ms). The maximal reduction in  $\text{Ca}^{2+}$  transient cycle length (by  $34 \pm 6\%$ ) was achieved in the following beat. Although the caffeine effects subsequently vanished, the CL remained slightly shortened even during washout (Fig. 2 A, and see Table S2). This prolonged caffeine effect could be due to its incomplete washout and/or possible CaMKII effects (CaMKII signaling might be activated during the initial caffeine-induced  $\text{Ca}^{2+}$  increase). Because we could not fully control washout in our experimental system and because our model does not describe CaMKII effects, we did not further study this effect, but focused mainly on several beats upon caffeine application. Note also that the beat-to-beat caffeine-induced changes in the  $\text{Ca}^{2+}$  transient cycle length are similar to the changes in  $T-90_c$  (Fig. 2 F) (We have previously demonstrated the crucial importance of  $T-90_c$ , reflecting SR  $\text{Ca}^{2+}$  refilling kinetics, for cardiac pacemaker cell function (27).)

## Numerical mechanisms of acute caffeine affect to shorten AP cycle length

We numerically tested three mechanisms of caffeine activation of RyR using different sets of model parameters: by increasing RyR sensitivity to lumenal SR  $[Ca^{2+}]$ ; by increasing RyR sensitivity to submembrane  $[Ca^{2+}]$ ; and by employing a combination of the above two changes. The results of our simulations are presented in Fig. 3. All three parameter sets reproduce an experimentally observed increase in diastolic  $Ca^{2+}$ , decrease in T-90<sub>c</sub>, and initial (first cycle) reduction in cycle length and increase in peak  $Ca^{2+}$  transient. However, only the SR  $Ca^{2+}$  sensitivity model of caffeine effect (*left columns* in Fig. 3) reproduces the experimentally observed transient change in peak cytosolic  $Ca^{2+}$  transients and cycle-length reduction over the next several subsequent cycles. Three existing pacemaker-cell models (Kurata et al. (16), the original Maltsev and Lakatta (17), and Severi et al. (18)) also failed to reproduce the dynamics of the peak cytosolic  $Ca^{2+}$  transient measured here (see Fig. S2).

Fig. 4 shows numerical model simulations that provide further mechanistic insights of the caffeine effect to acutely reduce CL in our proposed new model. These model simulations demonstrate that in response to spontaneous caffeine application, LCRs from the SR occur earlier and induce a larger and earlier inward  $I_{NCX}$  that, in turn, accelerates the DD, prompting the earlier occurrence of the next AP.

## The effect of flash-induced $Ca^{2+}$ release

We have recently demonstrated that NP-EGTA, a caged  $Ca^{2+}$  buffer, substantially slows the AP firing rate, and that flash-induced  $Ca^{2+}$  release from the buffer instantly reduces CL for several AP cycles (15) (see example of experimental recordings in Fig. 5, D–F). In this study we measured caffeine-induced  $Ca^{2+}$  transients (as a traditional measure of releasable  $Ca^{2+}$  within the SR) before and after NP-EGTA loading into single SANC. Loading of NP-EGTA reduced the caffeine-induced  $Ca^{2+}$  release by 15% (Fig. 5, A–C). Thus, before flash photolysis, the AP firing rate was slow and dysrhythmic (Fig. 5 D), likely due to the abnormally lower SR  $Ca^{2+}$  loading and interference of NP-EGTA (as a  $Ca^{2+}$  buffer) with  $Ca^{2+}$ -dependent processes.

To numerically simulate the effects of NP-EGTA on  $Ca^{2+}$  cycling dynamics, it was first necessary to estimate the intracellular NP-EGTA concentration and its effect to perturb SR release  $Ca^{2+}$ . The red curve in Fig. 6 A shows the relationship between intracellular NP-EGTA concentration and CL predicted by our proposed new model. The CL increased (phase 1) at an NP-EGTA concentration between 1 and 7 mM. The experimentally observed reduction in caffeine-induced  $Ca^{2+}$  release (Fig. 5 C) is in a good agreement with our modified model prediction of reduction of average network SR  $[Ca^{2+}]$  at 8 mM of NP-EGTA (Fig. 6 B). At an NP-EGTA concentration between 7 and 9 mM, the CL continued to increase and AP firing became dysrhythmic (phase 2 in Fig. 6 C). At still higher NP-EGTA

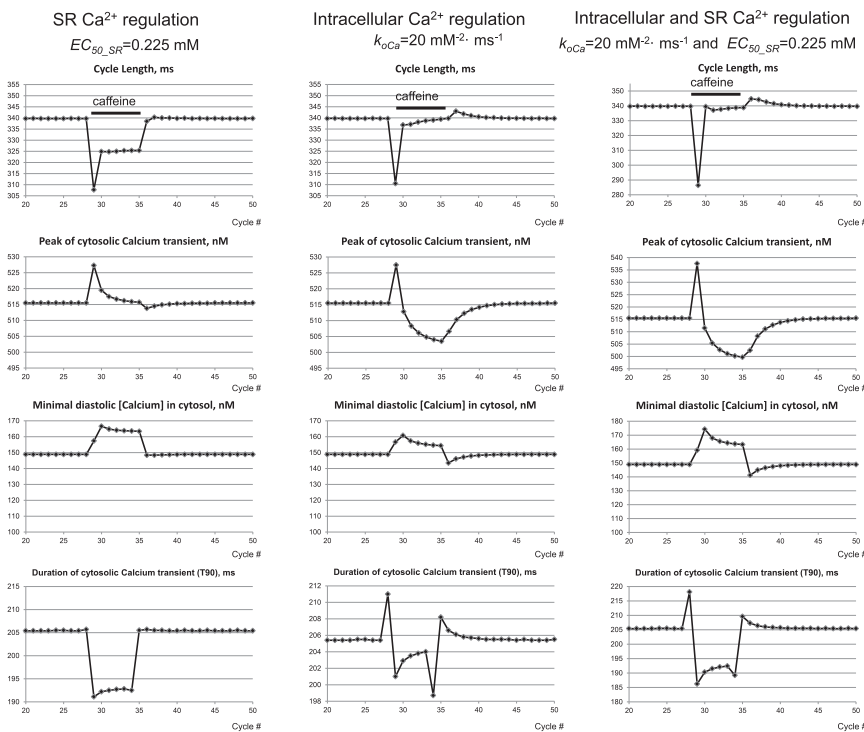


FIGURE 3 Numerical model simulations of SANC responses to acute caffeine application. We explored three different potential mechanisms of RyR activation by caffeine. (*Left column*) Increasing RyR sensitivity to lumenal SR  $[Ca^{2+}]$ ; (*middle*) increasing RyR sensitivity to submembrane  $[Ca^{2+}]$ ; and (*right*) a combination of the above two changes. Specific model parameter changes are shown at the top of each column.



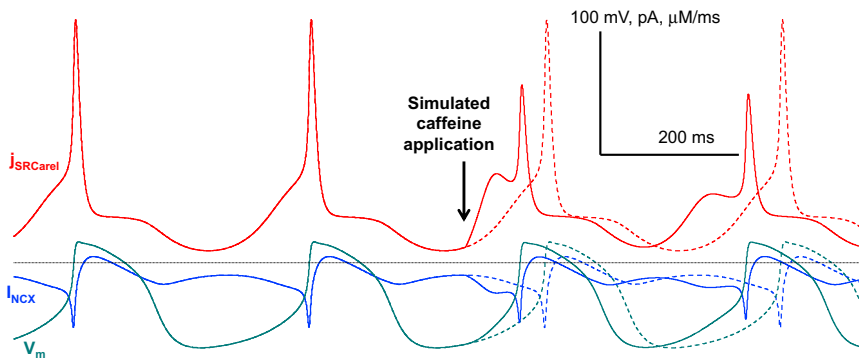


FIGURE 4 Numerical model simulation of the mechanism of the acute caffeine effect. Caffeine acutely increases diastolic  $\text{Ca}^{2+}$  release ( $j_{\text{SRCarel}}$ ), which accelerates diastolic depolarization ( $V_m$  trace) via activation of the  $\text{Na}^+/\text{Ca}^{2+}$  exchanger current ( $I_{\text{NCX}}$ ).

concentrations, AP firing ceased (phase 3). Our prior experimental data have shown that in response to NP-EGTA loading, the AP cycle length also increases and becomes dysrhythmic (15). Therefore, to reproduce the present experimental results, we estimated that the buffer concentration in the model should be  $\sim 8$  mM. This is a reasonable estimate: for example, in the study of Kurata et al. (16), intracellular concentration of EGTA (after cell loading with EGTA-AM) was estimated to be  $\sim 10$  mM. All three previous numerical models were less sensitive to NP-EGTA and none could reproduce the three phases of the NP-EGTA effect (Fig. 6 A, different colors).

Surprisingly, the CL in the model of Severi et al. (18) decreased as NP-EGTA concentration increased from 2 to 10 mM (Fig. 6 A, inset). Our more detailed examination revealed that this model cannot hold  $\text{Na}^+$  homeostasis:  $\text{Na}_i$  drops to 4.6 mM,  $\text{Ca}_{\text{sub}}$  to as low as 39 nM (not shown), and SR  $\text{Ca}^{2+}$  loading to 0.349 mM (i.e.,  $>3$  times) (see Fig. S3), which contradicts the experimental results (Fig. 5, A–C). Low intracellular  $\text{Na}^+$ , in turn, increases diastolic  $I_{\text{NCX}}$  (from 4.5 to 5.9 pA), which leads to AP rate acceleration (Fig. 6 A, inset), rather than the substantial rate-slowing observed experimentally, as NP-EGTA concentration increases (Fig. 5 D).

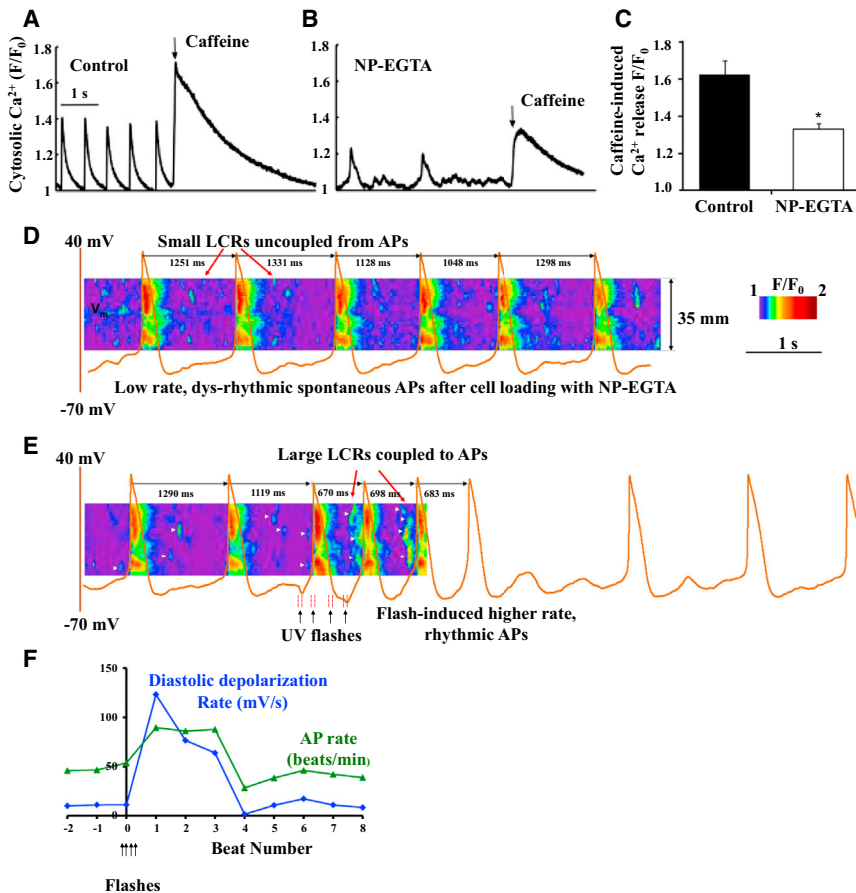
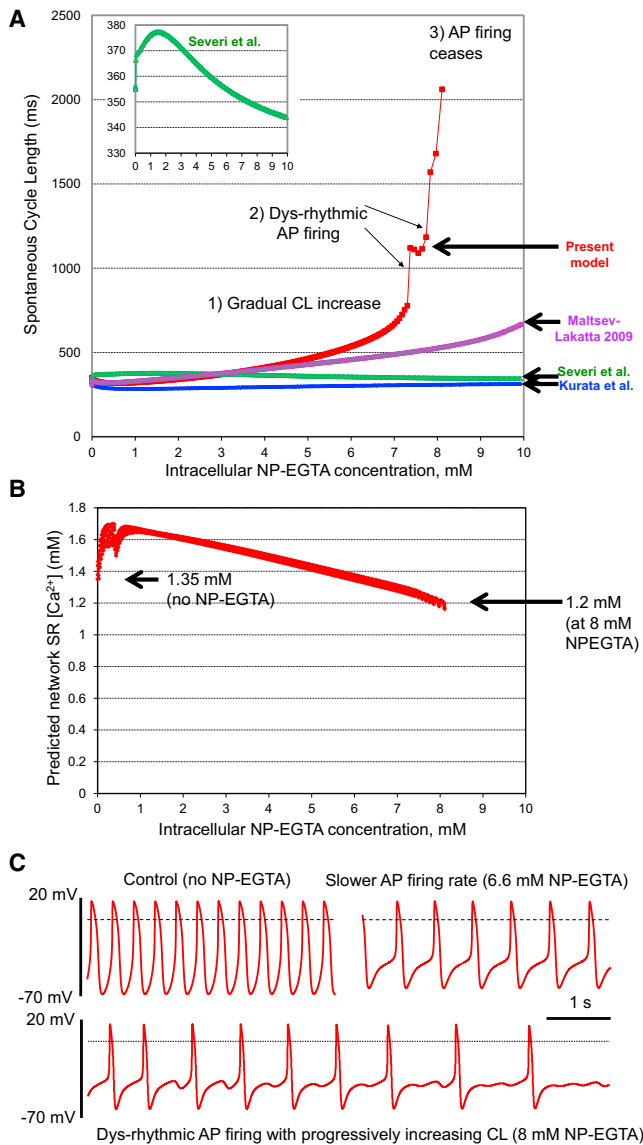


FIGURE 5 Photo-induced release of caged  $\text{Ca}^{2+}$  acutely reestablishes coupling of the  $\text{Ca}^{2+}$  clock and the M clock. (A and B) A representative example of effects of a rapid application of caffeine (indicated by the arrow) onto a SANC in control, or after loading SANC with NP-EGTA. (C) Average effects of NP-EGTA loading on the amplitude of caffeine-induced cytosolic  $\text{Ca}^{2+}$  transient ( $n = 9$  in control and in the presence of NP-EGTA). (D–F) (published previously in Yaniv et al. (15)) The effect of flash-induced  $\text{Ca}^{2+}$  release on membrane potential and simultaneous  $\text{Ca}^{2+}$  dynamics in our typical experiment in single rabbit SANC. (D) Before the flash, the  $\text{Ca}^{2+}$  buffer uncoupled LCRs (line-scan image) from APs, resulting in a slow, dysrhythmic AP firing rate. (E) After the last of four 50-ms UV flashes (solid arrows), large, synchronous LCRs emerge (small white arrows) and are coupled to the AP occurrence via an acute increase in DD rate, resulting in acute increase in AP firing rate (F).



**FIGURE 6** Simulations of the steady-state effect of NP-EGTA. (A) Predictions of different contemporary models of the change in AP cycle length as a function of intracellular NP-EGTA concentration. Only our proposed new model (i.e., the present model) predicts experimentally observed dynamics of the NP-EGTA effect: gradual CL increase and dysrhythmic AP firing. Although the model of Kurata et al. (16) is almost insensitive to intracellular  $Ca^{2+}$  buffering with NP-EGTA, the model of Severi et al. (18) shows CL decrease (rather than the increase observed experimentally) as [NP-EGTA] rises (see details in *inset*). (B) Prediction of our proposed new model for network SR  $Ca^{2+}$  loading under the same conditions as in panel A. (C) Representative examples of AP firing, simulated by our proposed new model for different concentrations of intracellular NP-EGTA.

### Approximation of photo-released $Ca^{2+}$ rate ( $j_{PPs}$ )

Upon application of UV flash, a small fraction of caged  $Ca^{2+}$  buffer (NP-EGTA) is hydrolyzed into photoproducts (PPs) with much lower affinities for  $Ca^{2+}$ . Because the  $Ca^{2+}$  unbinding rate for PPs is extremely fast (i.e., ~200,000 faster than that for NP-EGTA: 360 vs.

$0.0017 \text{ ms}^{-1}$ , as measured by Faas et al. (28)), we did not model the microsecond kinetics of  $Ca^{2+}$  release from PPs, but instead approximated the effect of the almost instantly released  $Ca^{2+}$  as a constant  $Ca^{2+}$  flux with a rate  $j_{PPs} = 1 \text{ } \mu\text{M/ms}$  into submembrane space and into cytosol (function of UV pulses intensity). Note that the exact fraction of NP-EGTA turning into PPs by flash remains unknown. Therefore we assigned the  $dCa_{sub}/dt$  part via flash-induced  $Ca^{2+}$  release ( $j_{PPs}$ ) to  $1 \text{ } \mu\text{M/ms}$  to reproduce the moderate effects of flash-induced  $Ca^{2+}$  signal increase observed in our control experiments (see the online supplement in Yaniv et al. (15)). For comparison, here we evaluated three benchmarks of  $dCa_{sub}/dt$  contributions using Eq. 13 and numerical model predictions for NP-EGTA-loaded SANC spontaneously firing APs:

1. The diastolic  $Ca^{2+}$  release flux predicted by the model (at  $-40 \text{ mV}$ )  $j_{SRCarel} = 26.6 \text{ } \mu\text{M/ms}$ :

$$\begin{aligned} (dCa_{sub}/dt)_{\text{diastolic release}} &= j_{SRCarel} \times V_{JSR}/V_{sub} \\ &= 26.6 \times 0.12 = 3.192 \text{ } \mu\text{M/ms}. \end{aligned}$$

2. The peak systolic  $Ca^{2+}$  release predicted by the model  $j_{SRCarel} = 75 \text{ } \mu\text{M/ms}$ :

$$\begin{aligned} (dCa_{sub}/dt)_{\text{systolic release}} &= j_{SRCarel} \times V_{JSR}/V_{sub} \\ &= 75 \times 0.12 = 9 \text{ } \mu\text{M/ms}. \end{aligned}$$

3. The peak  $I_{CaL}$  predicted by the model = 181 pA:

$$\begin{aligned} (dCa_{sub}/dt)_{\text{via peak } I_{CaL}} &= I_{CaL}/(2 \times F \times V_{sub}) \\ &= 26.7 \text{ } \mu\text{M/ms}. \end{aligned}$$

Thus, our simulated photo-release flux rate  $(dCa_{sub}/dt)_{\text{flash}} = j_{PPs}$  of  $1 \text{ } \mu\text{M/ms}$  represents only 31.3 and 11.1% fractions of the diastolic and systolic SR  $Ca^{2+}$  release benchmarks, respectively, and only 3.7% of the systolic peak  $I_{CaL}$ .

With this relatively small rate of  $Ca^{2+}$  release from the buffer (i.e., uncaging), our simulated  $4 \times 50 \text{ ms}$  flashes would require [NP-EGTA] to change by only  $200 \text{ } \mu\text{M}$  ( $4 \times 50 = 200 \text{ ms}$  of  $1 \text{ } \mu\text{M/ms}$  rate), i.e., by only a small fraction (~2.5%) of the total [NP-EGTA] of ~8 mM (at the time we applied flashes in the model). Therefore, we neglected this change in the [NP-EGTA] (model parameter  $CB\_Conc$ ) during the flashes. In turn, the effect of  $Ca^{2+}$  binding by PPs was not specifically modeled because the  $Ca^{2+}$  binding rate for PPs is the same as for NP-EGTA ( $CB\_on\_rate = 35 \text{ mM}^{-1} \times \text{ms}^{-1}$ ) as measured by Faas et al. (28).

Fig. 7 illustrates the coupled-clock model simulations of the experimentally measured changes in AP firing rate in response to the sequence of four photo-induced  $Ca^{2+}$  releases. The model simulations show that changes in intracellular  $Ca^{2+}$  can indeed regulate the duration of the same

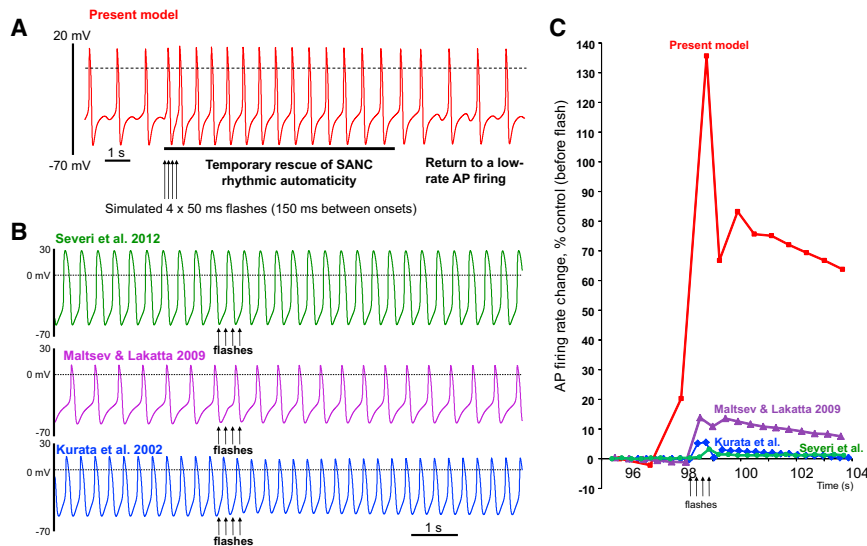


FIGURE 7 Simulations of the effect of flash-induced  $\text{Ca}^{2+}$  release. (A) Similar to experimental results in Fig. 5 F, the AP cycle length in our proposed new model simulation becomes temporarily reduced (i.e., rescued) after four 50-ms UV flashes (solid arrows). (B) In contrast, numerical simulations using different contemporary models fail to predict the AP cycle-length shortening observed experimentally. (C) Changes in AP firing rate after four 50-ms UV flashes predicted by the models.

spontaneous cycle in which it was changed, as well as several subsequent spontaneous AP cycles of SANC (the memory effect). Similar to the experimental data (Fig. 5 E), the initial effect of the flashes to markedly accelerate DD and acutely reduce cycle length after the termination of the last flash (between simulated beats 3 and 4 in Fig. 7 A) occurred at the same beat. After nine rhythmic APs, the effects of the flash waned, due to reestablishment of altered SR  $\text{Ca}^{2+}$  cycling dynamics by the caged buffer, and the SANC AP firing rate again became slower and dysrhythmic (both in the model and in the experiments; compare Figs. 5 E and 7 A). Our additional simulations revealed that three previous models had been less sensitive to flash-induced  $\text{Ca}^{2+}$  and could not reproduce the substantial decrease in the AP cycle length rate after the flashes (Fig. 7, B and C).

### Numerical mechanisms of the effect of photo-released $\text{Ca}^{2+}$ on the SANC AP firing rate

In our experiments, four 50-ms flashes were applied experimentally with a time interval of 150 ms between the flashes onsets (solid arrows in Fig. 5 E). The photo-released  $\text{Ca}^{2+}$  dramatically affects the DD slope and AP cycle length (Fig. 5 F). Simulations using our proposed new model reproduce the marked increase in DD slope after the flash (marked “DD acceleration” in  $V_m$  panel in Fig. 8). They also show that with each additional flash-induced  $\text{Ca}^{2+}$  release the SR load becomes increased and ultimately returns to basal level to  $\sim 1.35$  mM ( $\text{Ca}_{\text{free\_SR}}$  panel in Fig. 8), i.e., the level evaluated under normal conditions, before NP-EGTA (arrow, no NP-EGTA in Fig. 6 B). Concurrently, diastolic  $[\text{Ca}^{2+}]_{\text{subspace}}$  and  $I_{\text{NCX}}$  also increase,

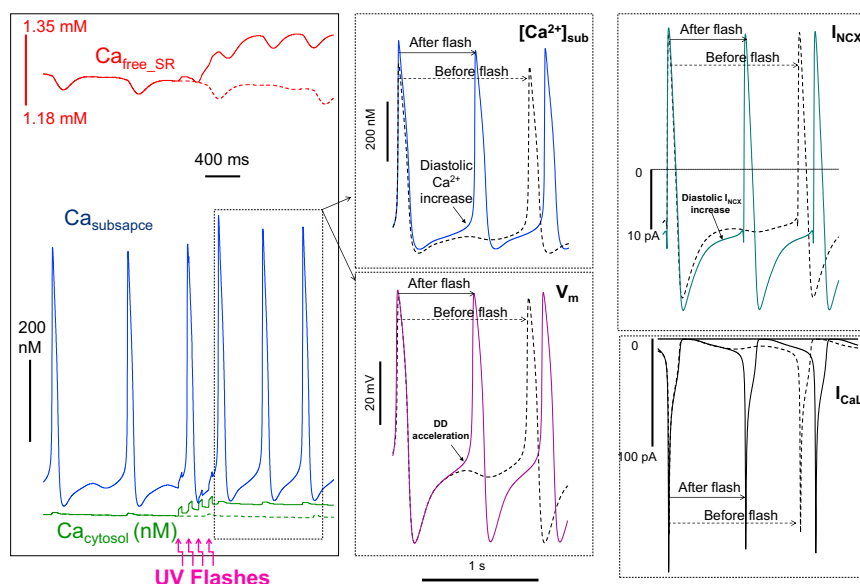


FIGURE 8 Numerical mechanisms that contribute to AP cycle-length shortening caused by photo-released  $\text{Ca}^{2+}$ . Predicted changes in response to photo-released  $\text{Ca}^{2+}$ , in the network SR  $[\text{Ca}^{2+}]$  ( $\text{Ca}_{\text{free\_SR}}$ ), cytosolic  $[\text{Ca}^{2+}]$  ( $\text{Ca}_{\text{cytosol}}$ ), submembrane  $[\text{Ca}^{2+}]$  ( $[\text{Ca}^{2+}]_{\text{sub}}$ ),  $\text{Na}^+/\text{Ca}^{2+}$  exchanger current ( $I_{\text{NCX}}$ ), membrane potential ( $V_m$ ), and L-type  $\text{Ca}^{2+}$  current ( $I_{\text{CaL}}$ ) are shown. To illustrate the difference, the predicted changes are compared with those in control simulations, i.e., those in which no flashes were applied (dashed lines).



driving DD acceleration that normalizes (i.e., rescues) the rate of rhythmic beating (*respective panels* in Fig. 8). This numerical model simulation reproduces the experimental observation of the emergence of large, abundant LCRs after the flash. In other words, the acute, transient, marked reduction in AP cycle length caused by the flash, was likely mediated in our experiments by its effects to markedly increase LCRs, which accelerated the DD via  $\text{Ca}^{2+}$ -dependent effects on sarcolemmal molecules (such as an increase in the diastolic  $I_{\text{NCX}}$ ).

Our additional model simulations (see Fig. S4) provided an insight into the memory effect observed experimentally (Fig. 5 E) and predicted by our proposed new model (Fig. 7 A): The flash-induced  $\text{Ca}^{2+}$  releases nearly-instantaneously elevate both cytosolic and SR  $\text{Ca}^{2+}$  levels (i.e., the released  $\text{Ca}^{2+}$  accumulates in the cytosol and within the network SR). Because NCX can extrude only a limited amount of  $\text{Ca}^{2+}$  each cycle, the intracellular  $\text{Ca}^{2+}$  levels remain elevated for several pacemaker cycles, which are characterized by a shorter CL. Thus, for the time period of those several cycles, the cell “remembers” the perturbation of its  $\text{Ca}^{2+}$  balance by flash-induced  $\text{Ca}^{2+}$  releases.

## DISCUSSION

Using two different acute perturbations, i.e., flash-induced  $\text{Ca}^{2+}$  release and caffeine-induced  $\text{Ca}^{2+}$  release, our experimental results and numerical model simulations provide strong evidence that changes in intracellular  $\text{Ca}^{2+}$  dynamics regulate the AP firing rate on a beat-to-beat basis. Specifically, we found that changes in intracellular  $\text{Ca}^{2+}$  within an AP cycle can regulate the duration of that AP cycle length, and this effect of spontaneous AP cycle length shortening can sustain for several cycles.

## Numerical mechanisms

Our numerical model simulations reproduce our proposed new experimental results and also predict that the instantaneous effect of  $\text{Ca}^{2+}$  regulation on SANC automaticity is produced via activation of  $I_{\text{NCX}}$  (Fig. 8). The memory effect observed experimentally for several subsequent cycles after flash-induced  $\text{Ca}^{2+}$  release in SANC, is accomplished in the model simulation via a change in SR  $\text{Ca}^{2+}$  pumping (see Fig. S4) to regulate SR  $\text{Ca}^{2+}$  loading, diastolic  $\text{Ca}^{2+}$  release, and diastolic  $I_{\text{NCX}}$ .

A brief application of caffeine substantially and acutely decreases the AP cycle length. Caffeine increases the open probability of RyR, and therefore more  $\text{Ca}^{2+}$  is released by the SR. In ventricular myocytes a low concentration of caffeine increases the frequency and decreases the amplitude of spontaneous  $\text{Ca}^{2+}$  release (29). In SANC, application of caffeine produced a transient increase in the amplitude of the systolic  $\text{Ca}^{2+}$  transient, and on the following beats the amplitude of the systolic  $\text{Ca}^{2+}$  transient

decreased (see Table S2), i.e., similar to ventricular myocytes (29). However, in SANC the increase in diastolic  $[\text{Ca}^{2+}]$  on the following beats is sustained, effecting a reduction of AP cycle length for several beats via activation of diastolic  $I_{\text{NCX}}$ . We compared three different numerical models of caffeine activation of RyR (Fig. 3) and discovered that the modified model that increases the sensitivity of RyR activation by luminal SR  $\text{Ca}^{2+}$  faithfully reproduces all changes in parameters of AP-induced  $\text{Ca}^{2+}$  transients measured experimentally. Therefore, similar to ventricular myocytes (25) and HEK-293 cells expressing RyR2 (30), a low concentration of caffeine likely affects the sensitivity of RyR activation by luminal SR  $\text{Ca}^{2+}$ . Because our experiments were performed under in vitro conditions in single cells, rather than in bilayers, permeabilized cells, or noncardiac HEK cells, we provide, for the first time to our knowledge, insights for the caffeine effect in intact cardiac cells.

Both caffeine- and flash-induced  $\text{Ca}^{2+}$  release accelerated the decay kinetics of cytosolic  $\text{Ca}^{2+}$  transient (assessed here as  $T_{90_c}$ ). Moreover, the increase in diastolic  $\text{Ca}^{2+}$  is correlated with the decrease in  $T_{90_c}$  (Fig. 2 F). It has been shown previously that  $T_{90_c}$  is highly correlated with the rate of SR  $\text{Ca}^{2+}$  refilling (27), which critically depends on SR pumping rate and  $\text{Ca}^{2+}$  available for pumping. Accelerated SR  $\text{Ca}^{2+}$  refilling, in turn, causes earlier and stronger diastolic  $\text{Ca}^{2+}$  releases and its attendant  $I_{\text{NCX}}$ . Therefore, caffeine and flashed-induced  $\text{Ca}^{2+}$  release accelerate the pacemaker cell rate partially via acceleration of SR  $\text{Ca}^{2+}$  pumping kinetics, which affects SR  $\text{Ca}^{2+}$  loading.

## Shortcomings of the contemporary pacemaker cell models

An important finding of the study is that existing advanced models of rabbit SA node cell, including Kurata et al. (16), the original Maltsev-Lakatta model (17), and its recent update by Severi et al. (18), failed to reproduce the long-term effect of  $\text{Ca}^{2+}$  buffering by NP-EGTA and the effects of the acute perturbations of  $\text{Ca}^{2+}$  dynamics (Figs. 6 and 7, and see Fig. S2). Although the model of Kurata et al. failed mainly because it does not feature a  $\text{Ca}^{2+}$  clock (i.e., spontaneous diastolic  $\text{Ca}^{2+}$  release), the two other models are coupled-clock types, and were expected to generate an adequate response. Their surprising failure indicates that these models did not describe important cardiac pacemaker mechanisms. What is the difference between these models and our proposed new model that reproduced the experimental results with critical perturbations of the system? In accord with the ideas of DiFrancesco (22) about the size of currents required for pacemaking and our detailed parametric sensitivity analysis (20), we excluded  $I_{\text{st}}$  and substantially reduced  $I_{\text{bNa}}$ . Note that Severi et al. (18) excluded these two currents completely. Compared to the model of Severi et al. (18), however, our proposed

new model keeps  $Na_i$  constant at 10 mM. Thus, these comparisons and our additional model simulations (see Fig. S3) can be interpreted to indicate that

1.  $Na^+$  homeostasis is likely more stable in reality than that described by Severi et al. (18); and
2. Additional experimental and numerical model studies are required to clarify  $Na^+$  regulation mechanisms in SANC.

Inadequate  $Na^+$  regulation (homeostasis) in contemporary models may also explain, in part, a recent paradoxical conclusion that  $I_f$  harms the robustness of the pacemaker cell system (31).

### Study limitations: local $Ca^{2+}$ control and plurality of caffeine targets

Although our simulations favor the idea of caffeine affecting luminal sensitivity of RyR activation, this result should be treated with some caution, because our model belongs to common-pool models and does not describe local  $Ca^{2+}$  regulation. Future modeling of local  $Ca^{2+}$  signaling in SANC will clarify this issue.

That caffeine targets molecules other than RyR, needs to be considered when delineating the boundaries of our interpretation of caffeine experiments. Caffeine can act as a phosphodiesterase inhibitor, and therefore it may increase PKA/cAMP that might contribute to the experimentally observed effect on AP firing rate (32). The kinetics of the phosphodiesterase inhibition by caffeine and kinetics of its effect on the downstream targets remain, however, unknown,

$I_K$  in the rabbit SAN consists mainly of  $I_{Kr}$  and not  $I_{Ks}$  (33). However, the contribution of  $I_{Ks}$  to the spontaneous AP firing rate substantially increases during  $\beta$ -adrenergic stimulation (34). Because the macromolecular complex producing  $I_{Ks}$  may contain phosphodiesterase (35), inhibition of phosphodiesterase by caffeine can also increase  $I_{Ks}$ . However, under basal conditions (as in our study), the role of  $I_{Ks}$  in response to caffeine is likely insignificant.

It was shown in smooth muscle of the oviduct that its long exposure (of ~30 s) to caffeine (in the concentration range used in this study) activates the  $K_{ATP}$  channel (36). In addition, a  $K_{ATP}$  channel opener slows the pacemaker activity of SANC (37). However, in our experiments, spritzing a low concentration of caffeine decreased the CL rather than increased it. Therefore, the opening of  $K_{ATP}$  channels is not a major target of caffeine in our conditions. However, higher concentrations of caffeine eliminate the spontaneous AP firing (Fig. 5). Specifically, we previously found that a decrease in spontaneous AP firing is associated with a reduction in cellular ATP (38). Because  $K_{ATP}$  channels become open in response to a decrease in intracellular ATP, only a high concentration of caffeine or long-time exposure to caffeine may open  $K_{ATP}$  channels in SANC, similar to smooth muscle of the oviduct.

Finally, it has been shown that a long exposure to caffeine, at similar concentrations that were used here, enhances the L-type current and  $I_f$  amplitude (39). However, how quickly these channels become affected by caffeine remains unknown. Future experiments are needed to identify additional plausible targets of caffeine.

### SUMMARY

Our results support the coupled-clock hypothesis of cardiac pacemaker cell function, i.e., SANC under normal physiological conditions operates as a result of mutual entrainment of an SR-based intracellular  $Ca^{2+}$  oscillator ( $Ca^{2+}$  clock) and a cell-membrane-based voltage oscillator (M clock) that interact with each other on a beat-to-beat basis. We show that this mutual entrainment is indeed very rapid (actually almost instantaneous) and that the  $Ca^{2+}$  clock, generating diastolic  $Ca^{2+}$  release, regulates the M clock on a beat-to-beat basis. This quick effect (and clock entrainment) is explained by the coupling of  $Ca^{2+}$  signals to the M clock via NCX, an ion exchanger that generates an inward current almost instantly regulated by  $Na^+/Ca^{2+}$  gradients during the DD. Our proposed new model simulation of the SR memory effect, in turn, suggests that the diastolic SR  $Ca^{2+}$  release depends not only on  $I_{CaL}$ -mediated  $Ca^{2+}$  influx of the prior cycle, but likely of several (four to nine) prior cycles, and this is an important factor that confers robustness the coupled-clock system. Because our proposed new numerical model (which has constant  $Na^+$ ) uniquely reproduces the experimental data, whereas other contemporary models (which featured  $Na^+$  dynamics) failed to reproduce the data, our newly gained knowledge about  $Na^+$  homeostasis in SANC is likely incomplete and requires additional experimental studies and numerical modeling approaches.

### SUPPORTING MATERIAL

Four figures, two tables and Numerical Model Details are available at [http://www.biophysj.org/biophysj/supplemental/S0006-3495\(13\)00971-5](http://www.biophysj.org/biophysj/supplemental/S0006-3495(13)00971-5).

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